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VERIFICATION OF TRANSLATION

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I verify that the attached English translation is a true and correct translation made by me of the attached documents in the German language;

I further declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment or both under Section 1001 of Title 18 of the United States Code and that such willful false statements may jeopardize the validity of the application or any patent issued thereon.

Date: May 15, 2003

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Method of and apparatus for carrying out signal-processing
 consideration of a measurement signal related to
 the respiration activity of a person

5 The invention concerns a method of and an apparatus for carrying
 out signal-processing consideration of a measurement signal related to
 respiration activity, for example the respiratory gas flow, in particular for
 matching pressure regulation in the administration of a breathable gas at a
 pressure level which at least in phase-wise manner is above the ambient
 10 pressure, and generally for the diagnosis and/or therapy of sleep-related
 breathing disorders.

 To treat sleep-related breathing disorders it is known to supply a
 patient with a respiratory gas, in particular ambient air, at a pressure level
 which is above the ambient pressure level at least in phase-wise manner.
 15 The administration of the respiratory gas at an increased pressure level
 makes it possible to implement pneumatic splinting in the region of the
 upper respiratory tracts, whereby it is possible to preclude any obstructions
 in that respiratory tract region in a physiologically highly compatible
 fashion.

20 Particularly good compatibility of the supply of the respiratory gas at
 an elevated pressure level is achieved if the respiratory gas pressure is set
 to a pressure which is as low as possible and which is only sufficient for
 obstruction prevention or obstruction limitation. It is known to implement
 setting of the instantaneously required respiratory gas pressure, having
 25 regard to the evaluation results of signal-processing consideration of the
 instantaneous respiratory gas flow, by means of an electronic pressure
 regulating device which is integrated into a CPAP unit. The instantaneous
 respiratory gas flow can be detected in particular by volume flow sensors,
 for example measurement orifices.

30 In the case of CPAP units with automatic pressure matching the
 electronic pressure regulating device is configured with the aim that the
 respiratory gas pressure required is afforded with an adequate level of
 certainty, but on the other hand the dynamics of the variation in pressure

are so slight that the sleep pattern of the patient is not noticeably adversely affected by the changes in the respiratory gas pressure. Adverse effects can occur in particular if comparatively high respiratory gas pressure levels are temporarily set.

5 The object of the present invention is to provide ways with which it is possible to achieve electronic evaluation, which is accurate with a high degree of probability, of a signal that is representative in respect of respiration activity, so that, based on that evaluation, the physiological state of a patient can be accurately determined and/or the respiratory gas
10 supply, in particular the respiratory gas pressure, can be matched to the instantaneous physiological demands in an improved manner.

 In accordance with the invention that object is attained in that, in the context of signal-processing consideration of a measurement signal which is indicative of the respiratory gas flow, consideration results are obtained
15 which permit differentiation between obstructive and central breathing disorders.

 In that way it is advantageously possible, in connection with detection of the instantaneous respiratory gas flow, to implement an analysis of trends, by virtue of which it is possible to carry out the
20 measures which are most suitable for eliminating or preventing an instantaneous or impending breathing disorder, in particular involving matching the pressure regulating characteristics.

 In accordance with a particularly preferred embodiment of the invention signal-processing consideration is effected in such a way that the
25 inspiration time and the expiration time for successive breaths is detected thereby. By determining the ratio of the inspiration time and the expiration time and by considering the variation in respect of time of those ratios, it is possible to recognise a trend as to whether imminent breathing disorders or breathing disorders which already exist are caused obstructively and/or
30 centrally.

 In particular in combination with that measure, or also alternatively thereto, it is also possible to obtain information in respect of an existing or imminent disorder phase from comparative consideration of successively

occurring changes in properties of the derivatives and in particular the first derivative of the respiratory gas flow in the region of the breathing phase change.

5 The ratio of inspiration time I_x to expiration time E_x can be used to describe breathing disorders. In particular a trend in the variation in the duration of the inspiration time with respect to the expiration time can give an indication of an imminent obstruction in the upper respiratory tracts. Furthermore, consideration of the ratio of inspiration time I_x to expiration time E_x in a trend analysis procedure can contribute to distinguishing
10 obstructive from central apneas.

Exact measurement of the respiratory gas flow 'flow curve' is particularly advantageous.

The ratio of inspiration to expiration can be referred to as the duty cycle and represents an information carrier for assessment of the
15 respiratory flow disturbances in the upper respiratory tracts. If flow limitations actually occur, the inspiration time seemingly increases. The nasally measured resistance of the upper respiratory tracts in contrast remains unchanged. If it is assumed that the breathing minute volume remains constant, it is possible to deduce a relationship between the
20 volume flow, the inspiration duration and the breath duration. (The breath minute volume is equal to the volume flow multiplied by the inspiration time and divided by the breath duration.)

In particular in combination with that measure or also alternatively thereto it is also possible to obtain information for an existing or imminent-
25 disturbance phase from comparative consideration of successively occurring changes in properties of the derivatives of the - or within the - respiratory cycles, in particular the first derivative of the respiratory gas flow in the region of the breathing phase change.

30 Consideration of the differential can be directed to the beginning of the inspiration cycle and/or to the end of the inspiration cycle and also to consideration of the curve shape during the inspiration cycle.

The average gradient can be calculated in simple form for intervals which extend for example over 10% of the time duration of the respective breathing phase.

5 The gradient (for example the maximum gradient at the phase change) can also be calculated floatingly within a window over the inspiration cycle.

The trend analysis in particular in respect of the nature and constitution of the respiratory drive is preferably implemented having regard to/with the inclusion of the signal evaluation results set forth
10 hereinafter:

- max. peak flow during the inspiration cycle
- the breath volume
- the inspiration time, and
- the second derivative of the measured flow curve.

15 In accordance with a further aspect of the invention signal-processing consideration is effected on the basis of consideration of the differential at the beginning of the expiration cycle or at the end of the expiration cycle respectively. The differential can be calculated in a simple form over an interval of for example 10% at the beginning of the expiration
20 cycle and after the expiratory maximum flow or computed floatingly over the expiration cycle. Evaluation can advantageously be effected in a similar fashion to that described hereinbefore, with the inclusion of the maximum peak flow during the expiration cycle, the breath volume and/or the expiration time and/or the second derivative (curvature) of the measured
25 flow curve during the expiration cycle. The evaluation procedure also makes it possible to afford information about the nature and the constitution of the upper respiratory tracts.

The flattening of the respiratory flow curve during the inspiration cycle can be interpreted in accordance with the model of the Starling
30 resistor as a flow limitation. Consideration of the configuration of the curve shape during the inspiration cycle in an interval between for example 10% after the beginning of the inspiration cycle and 10% before the end thereof can advantageously provide information about the elastic properties of the

upper respiratory tracts. It is also possible in that way to draw a conclusion about the Pcrit-value (the pressure at which the upper respiratory tracts close).

5 The signal processing procedure advantageously embraces in particular analysis of the number of local maxima and minima, the amplitude of the local maxima and minima, the sequence of the magnitude of the amplitudes of local maxima and minima and the frequency involved in the sequence of the local maxima and minima.

10 In accordance with a further aspect of the present invention the signal processing procedure according to the invention preferably also includes spectral consideration and consideration in respect of amplitude of a snoring signal and on the basis thereof can furnish information about the nature of the elastic properties of the upper respiratory tracts and possibly about the nature and location of the closure in the upper respiratory tracts.

15 In accordance with a particular aspect signal-processing evaluation and the trend analysis based thereon are effected on the basis of combined consideration of at least two parameters as specified hereinafter. Trend analysis is preferably based on consideration of the variation in the ratios of the parameters when considered in combination:

20 inspiration time
expiration time
breath duration and breath frequency
breath volume during the inspiration cycle
breath volume during the expiration cycle
25 first differential and second differential of the respiratory flow
amplitudes of local maxima and local minima
frequency of local maxima and local minima
inflexion points
maximum inspiratory flow and maximum expiratory flow.

30 Signal-processing consideration of the above-specified parameters can give information about the following:

- the nature of the upper respiratory tracts inter alia for distinguishing between central and obstructive apneas

- the elastic properties of the upper respiratory tracts (restoring modulus, modulus of elasticity)
- the location of an obstruction
- the degree of severity of a sleep apnea
- the Pcrit-value.

Further details and features will be apparent from the description hereinafter with reference to the drawing in which:

Figure 1 shows a part of a respiratory gas flow chart to explain signal-processing consideration on the basis of ascertaining the ratios of the inspiration duration to the expiration duration for successive respiratory cycles,

Figure 2 shows a part of a respiratory gas flow chart to explain signal-processing consideration on the basis of consideration of the change in the curve shape features of successive inspiration cycles,

Figure 3 shows a part of a respiratory gas flow chart to explain signal-processing consideration on the basis of consideration of the change in the curve shape features of successive expiration cycles, and

Figure 4 shows a part of a respiratory gas flow chart to explain signal-processing consideration on the basis of evaluation of curve shape features within intervals in successive inspiration cycles.

Figure 1 shows a part from a respiratory gas flow chart for explaining signal-processing consideration on the basis of ascertaining the ratios of the inspiration duration to the expiration duration for successive respiratory cycles.

The ratio of inspiration time I_x to expiration time E_x and in particular the variation thereof for successive respiratory cycles represents information which is indicative in respect of the occurrence of breathing disorders. In particular a trend in the change in the duration of the inspiration time with respect to the expiration time can give a pointer to imminent obstruction in the upper respiratory tracts. In addition consideration of the ratio of inspiration time I_x to expiration time E_x in a trend analysis can contribute to differentiating obstructive from central apneas. Measurement of the respiratory gas flow, which is as accurate as

possible, and therewith possible depiction of the flow curve is advantageous.

The ratio of inspiration to expiration can be referred to as the duty cycle and represents an information carrier for assessment of the respiratory flow disturbances in the upper respiratory tracts. If flow limitations actually occur, the inspiration time seemingly increases. The nasally measured resistance of the upper respiratory tracts in contrast remains unchanged.

If it is assumed that the breathing minute volume remains constant, it is possible to deduce a relationship between the volume flow, the inspiration duration and the breath duration. (The breath minute volume is equal to the volume flow multiplied by the inspiration time and divided by the breath duration.)

Figure 2 shows a part of a respiratory gas flow chart to explain signal-processing consideration on the basis of consideration of the change in curve shape features of successive inspiration cycles. The chart in Figure 2 illustrates the mean gradient ascertained by way of the first derivative of the respiratory gas flow at the beginning of the inspiration cycle and at the end of the inspiration cycle respectively. That mean gradient is calculated in a simple form over for example a 10% interval or calculated floatingly over the inspiration cycle. Further curve shape features that can be taken into consideration are in particular the extreme values of the respiratory gas flow (peak flow during the inspiration cycle) and/or the breath volume and/or the inspiration time and/or the second derivative of the detected flow curve. Evaluation of those curve shape features - and in particular consideration of the variation thereof - permits information to be obtained about the nature and the constitution of the breathing drive, that is to say the instantaneous physiological state of the patient or the physiological state which prevails shortly.

Figure 3 shows a part from a respiratory gas flow chart for explaining signal-processing consideration on the basis of consideration of the change in curve shape features of successive expiration cycles, in particular in the form of evaluation of the differential at the beginning of the expiration cycle

or at the end of the expiration cycle respectively as can be ascertained in a simple form for example for a 10% interval at the beginning of the expiration cycle and after the expiratory maximum flow or floatingly over the expiration cycle.

5 Similarly as specified for Figure 2, in this case also further curve shape features which can be taken into consideration are in particular the extreme values of the respiratory gas flow (peak flow during the expiration cycle) and/or the breath volume and/or the expiration time and/or the second derivative of the detected flow curve. Evaluation of those curve
10 shape features - and in particular consideration of the variation thereof - permits information to be obtained about the nature and the constitution of the breathing drive, that is to say the instantaneous physiological state of the patient or the physiological state which prevails shortly.

Figure 4 shows a part of a respiratory gas flow chart to explain a
15 signal-processing consideration procedure on the basis of evaluation of curve shape features with intervals in successive inspiration cycles.

The flattening of the respiratory flow curve during the inspiration cycle can be interpreted (in accordance with the model of the Starling resistor) as a flow limitation. Consideration of the pattern of the curve
20 shape during the inspiration cycle in an interval between for example 10% after the beginning of the inspiration cycle and 10% before the end thereof gives information for example about the elastic properties of the upper respiratory tracts.

This analysis also makes it possible to draw conclusions about the
25 Pcrit-value (pressure at which the upper respiratory tracts close).

In carrying out a trend analysis procedure in particular the following evaluation intermediate results are advantageously taken into consideration:

- number of local maxima and minima
- 30 - the amplitude of the local maxima and minima
- the sequence of the magnitude of the amplitudes of local maxima and minima,
- the frequency in the succession of the local maxima and minima

- curve shape in an interval during the inspiration cycle
- length of the intervals.

Spectral consideration and consideration in respect of amplitude of a snoring signal can further provide information about the nature of the elastic properties of the upper respiratory tracts and about the location and nature of the closure in the upper respiratory tracts.

The invention is not limited to the examples of use described hereinbefore. It can be employed in particular in controlling respiratory gas pressure and matching pressure regulation in a CPAP-unit by using a suitably configured signal processing device. It can also be employed in regard to time-displaced evaluation of a series of measurement data and in that situation permits visualisation of obstructively or centrally caused phases of disturbed respiration. The invention can also be used in conjunction with a pneumotachograph generally for investigating the sleep breathing of a patient without in that respect any disturbances of obstructive nature having to be simultaneously eliminated directly by a respiratory gas supply at increased pressure.